

# Influence of the boundaries in imaging for damage localization in 1D domains

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# Detection and Localization of Damage

- Usually based on response recordings at a number of sensors to monitor structural integrity<sup>1</sup>
- Detection : comparison of recordings to a reference (undamaged) state
- Localization : Inverse Problem usually ill-posed
- Solution : *Time-Reversal* (TR) computational tool introduced by Fink et. al.<sup>2</sup>
- Achieves refocusing of the wave on the source
- Sending back the recorded signals but reversed in time
- Two step approach
  - Forward step
  - Backward step

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1. GE Stavroulakis, (2000) Inverse and crack identification problems in engineering mechanics  
2. Fink et. al., (2000) Time-reversed acoustics

# Time Reversal and applications

- TR is a physical process
- It exploits the time reversibility (based on spatial reciprocity and time reversal invariance) of linear wave equations
- Robust and Simple technique for source localization
- Has been applied in Acoustics<sup>3</sup>, Elastodynamics<sup>4</sup>, Electromagnetism, Hydrodynamics etc.
- Finds several applications in medicine, telecommunications, underwater acoustics, seismology, engineering structures, etc.
- TR can be used for scatterer localization
- The fundamental idea of TR can be exploited to develop different imaging techniques

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3. L Borcea, G Papanicolaou, C Tsogka and J Berryman, (2002) Imaging and time reversal in random media

4. D Givoli, (2014) Time Reversal as a Computational Tool in Acoustics and Elastodynamics

# In the present work

- Acoustic medium in an 1D bounded domain
- Description of the numerical implementation of TR
- Utilization of the Green's function of the Helmholtz equation to apply imaging techniques based on TR
- Investigation of the influence of the boundaries using modal expansion of the Green's function
- Investigation of the influence of the total experiment time  $T$
- Demonstration of numerical examples
- Proposition of techniques to improve the quality of the image and the SNR
- Indicative demonstration of a 2D example

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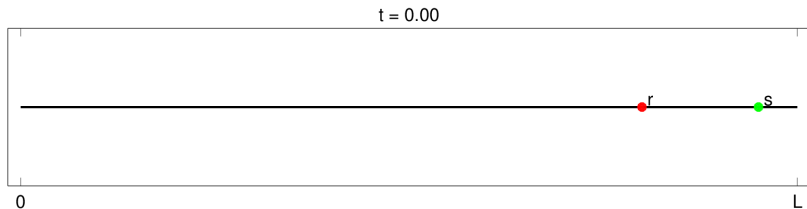
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- Simulated Numerically using a finite element method
- Wave propagation model

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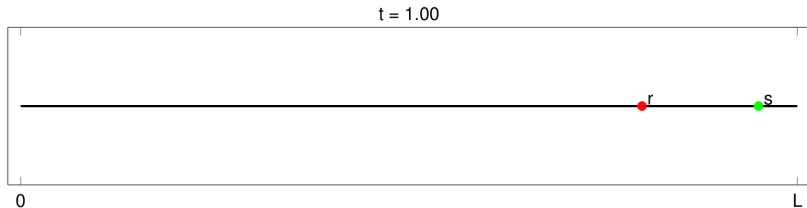


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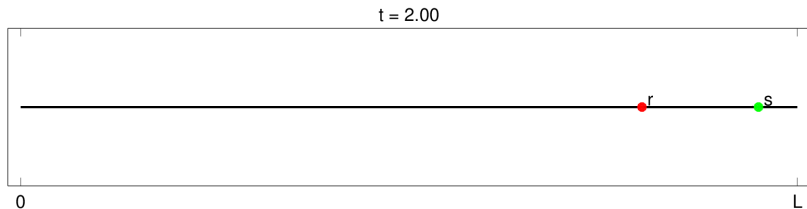


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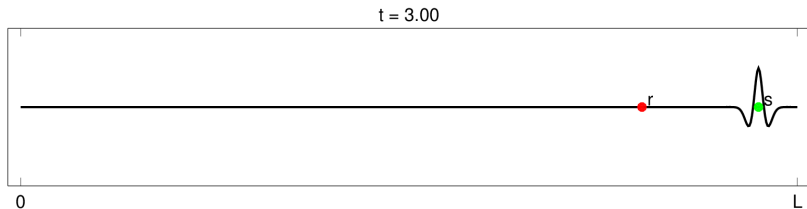


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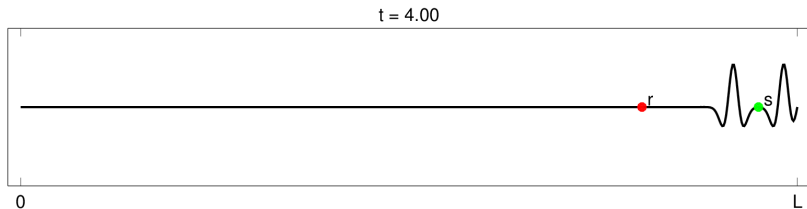


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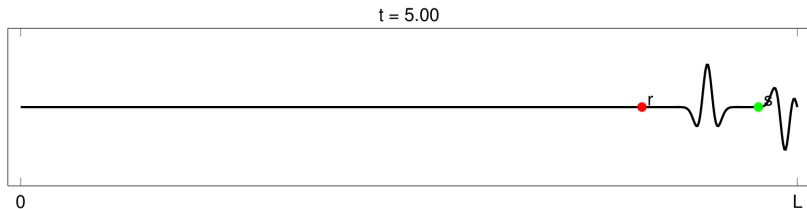


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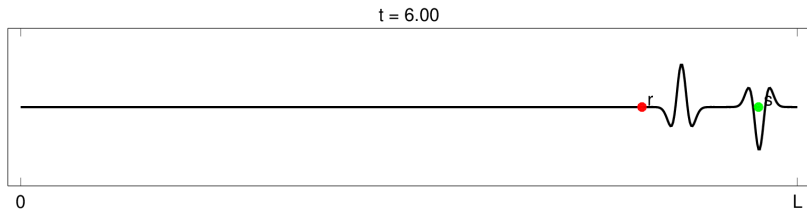


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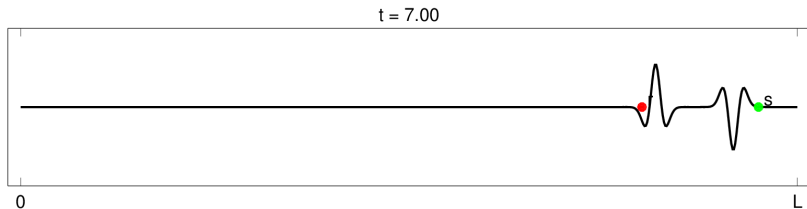


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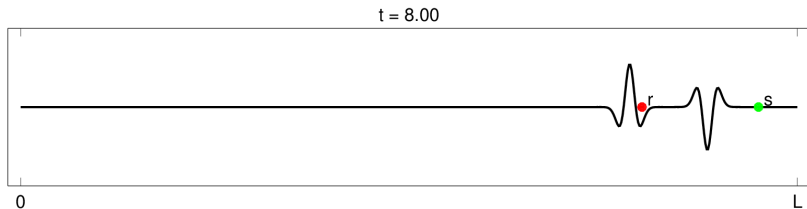


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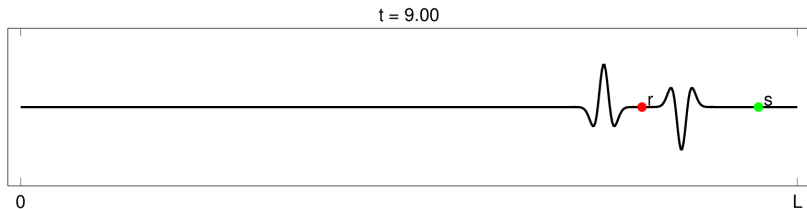


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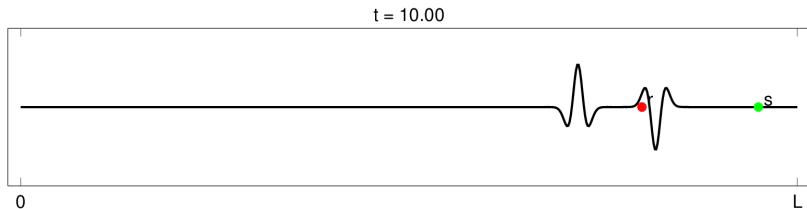


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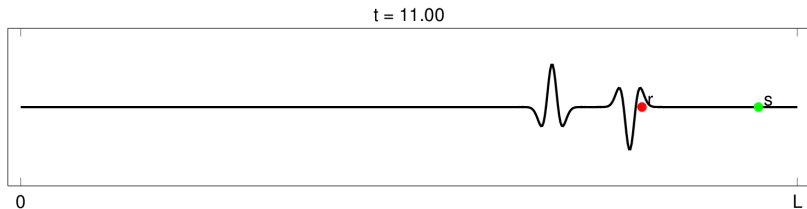


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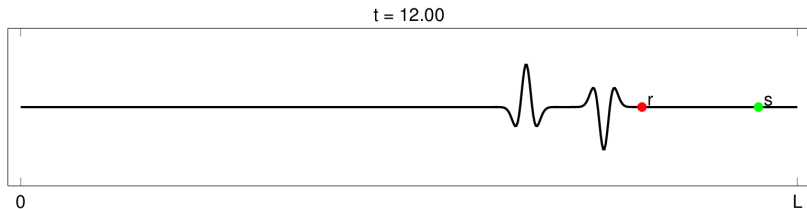


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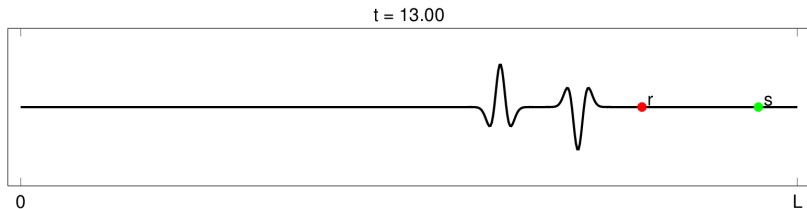


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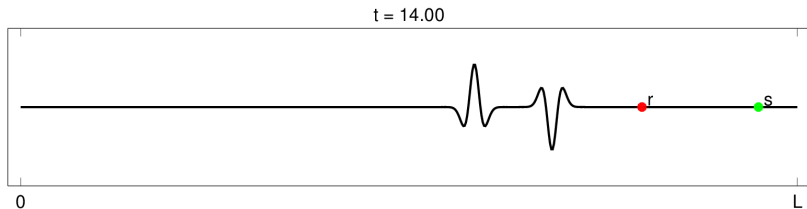


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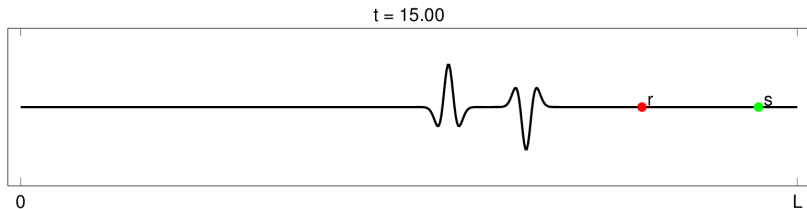


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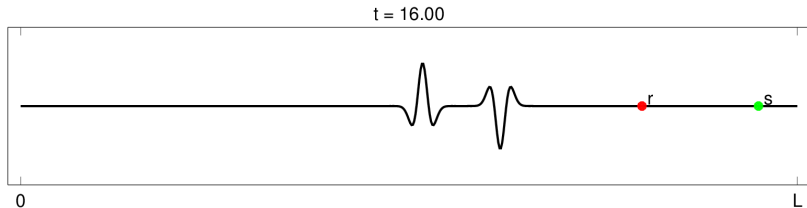


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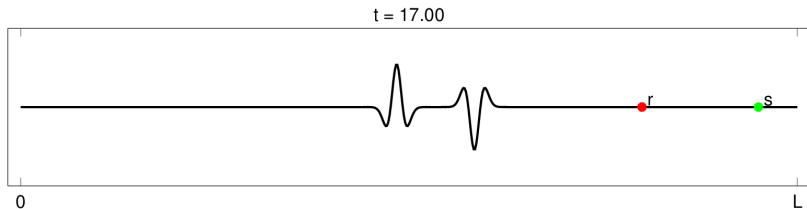


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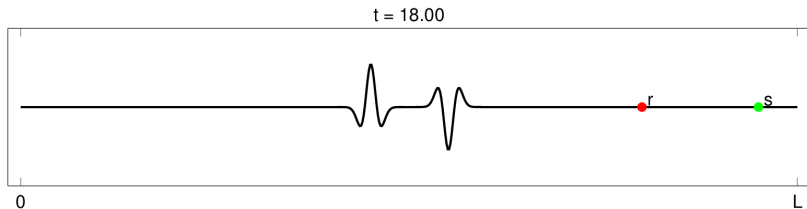


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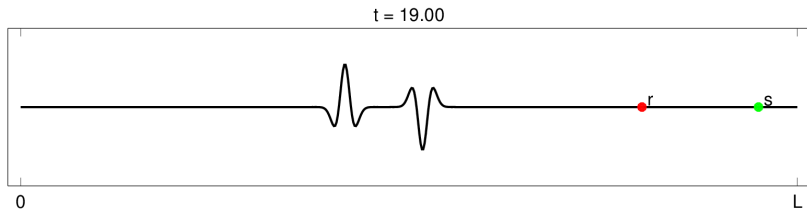


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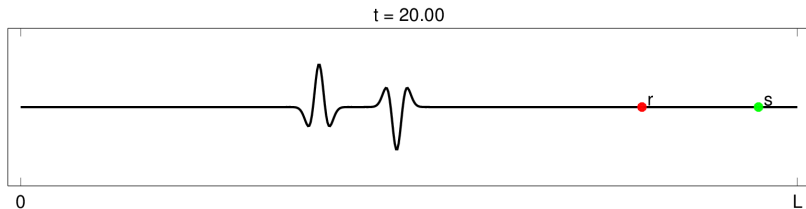


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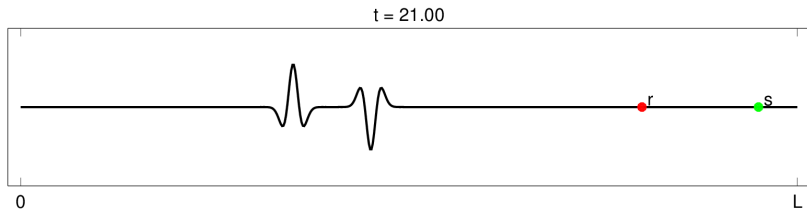


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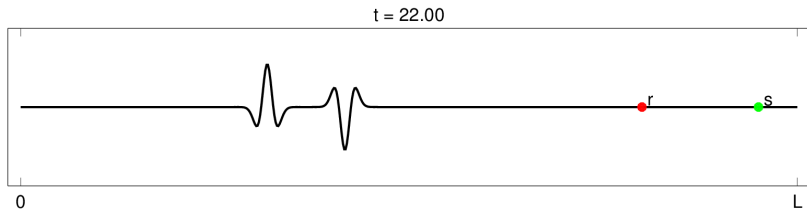


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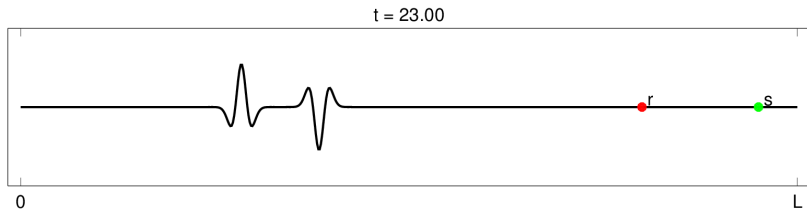


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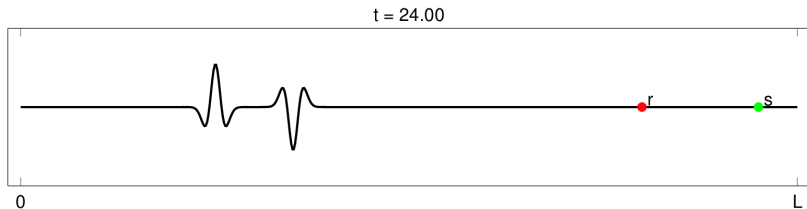


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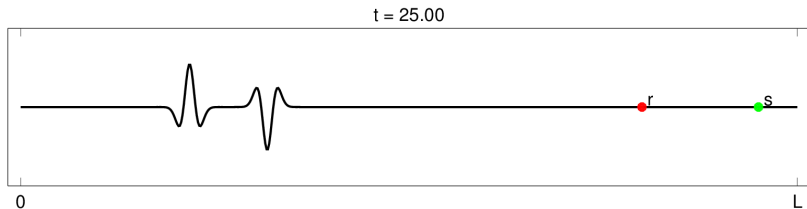


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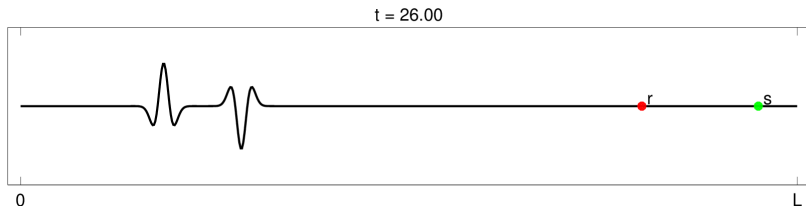


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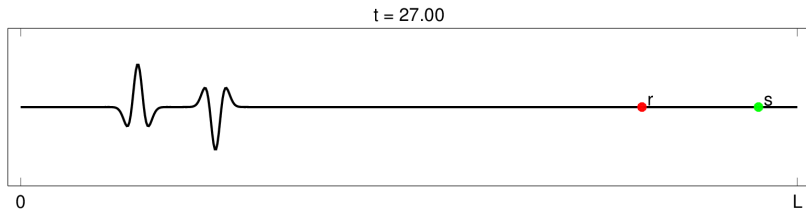


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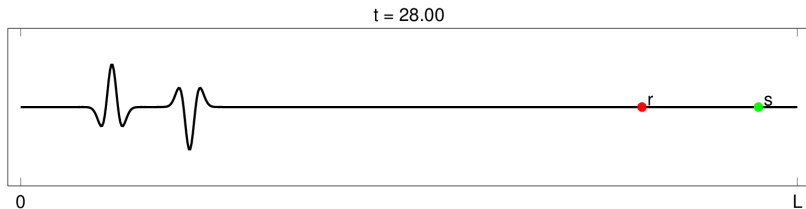


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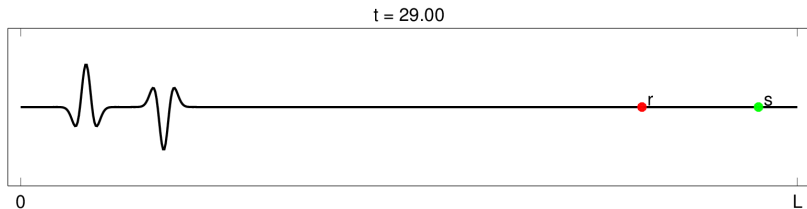


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- Excitation function  $f(t)$  is a Ricker pulse centered at a known  $t_0$
- The response  $p(x_r, t)$  is being recorded during total time  $T$

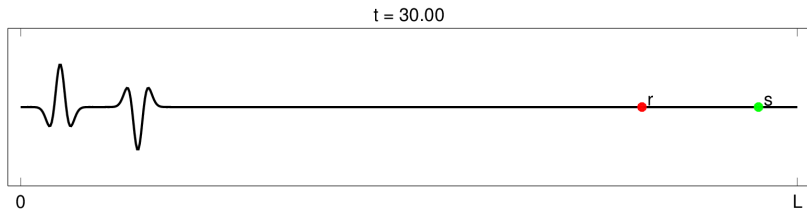


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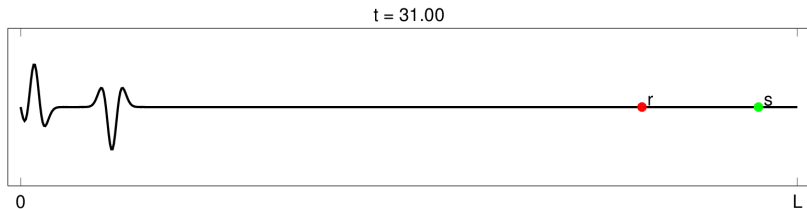


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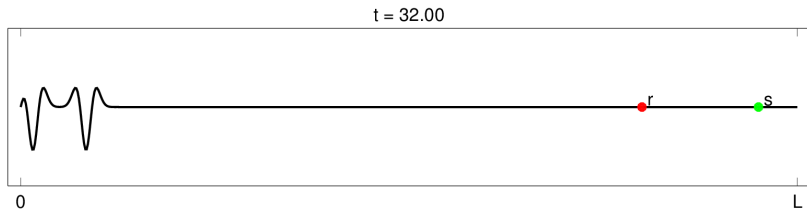


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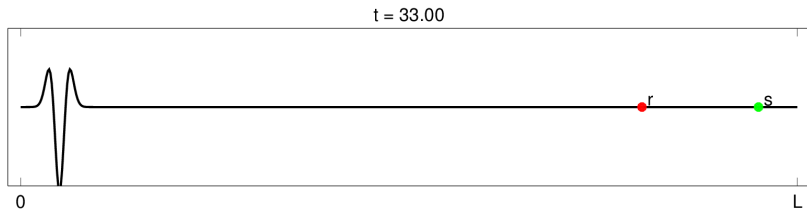


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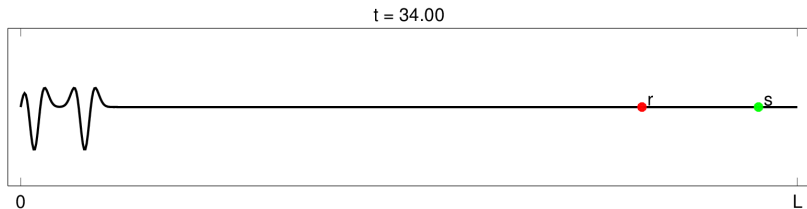


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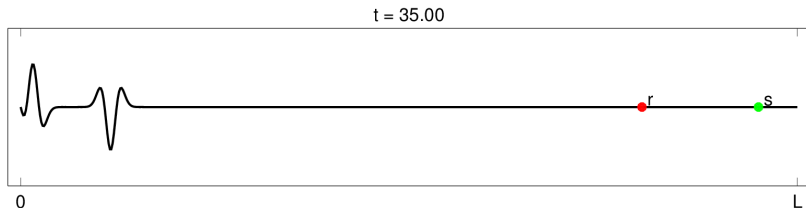


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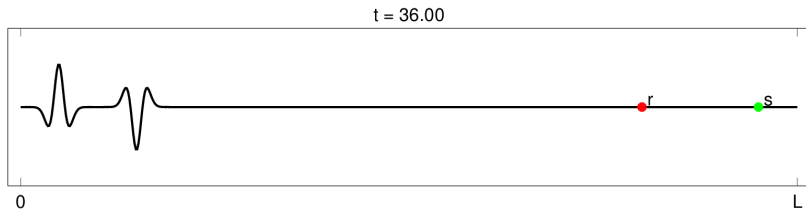


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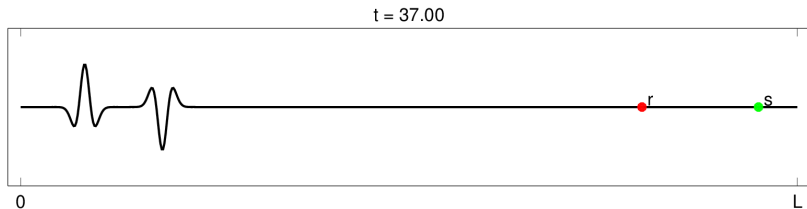


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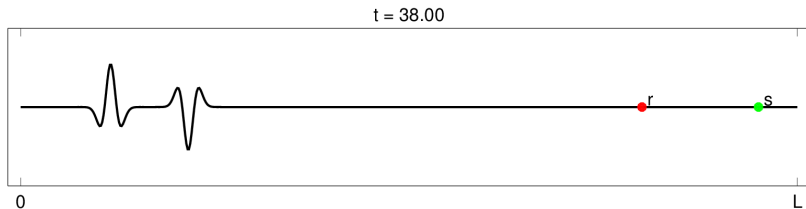


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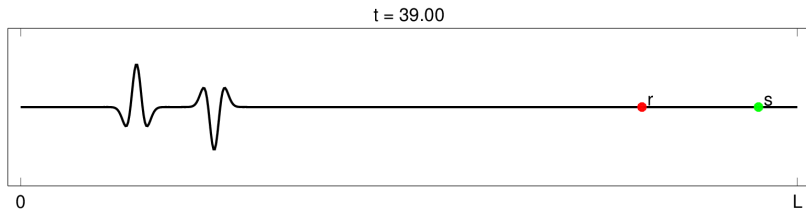


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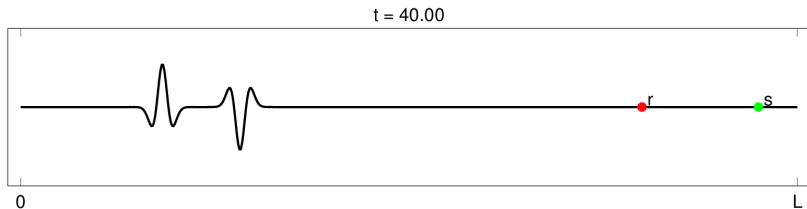


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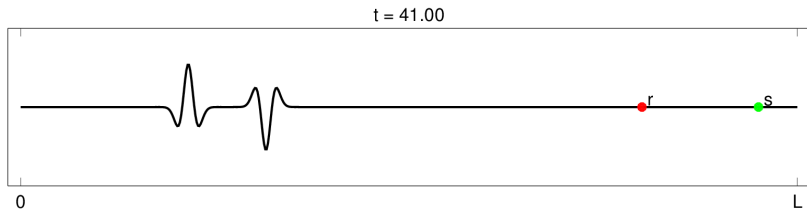


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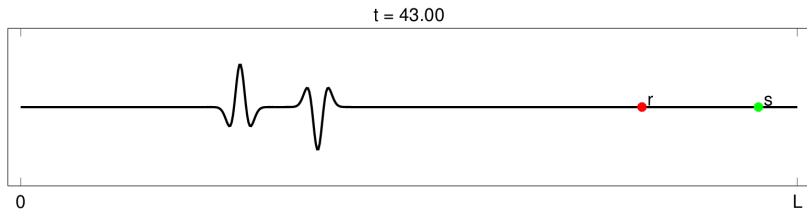


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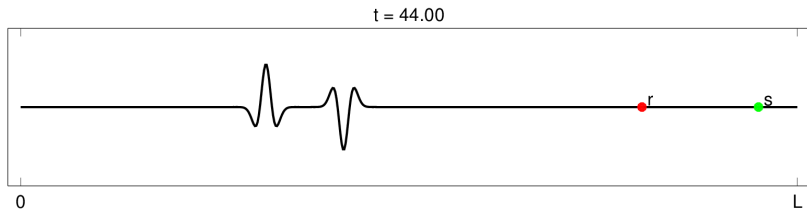


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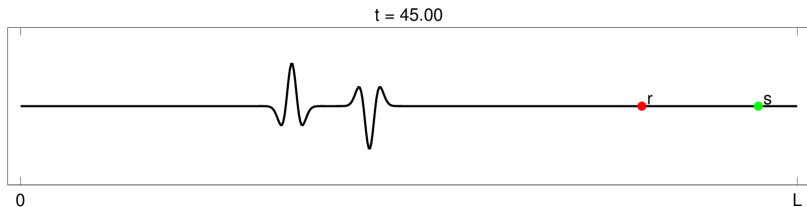


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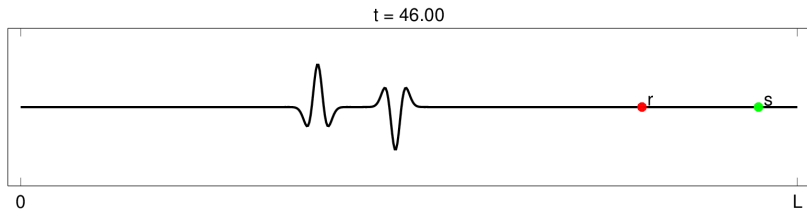


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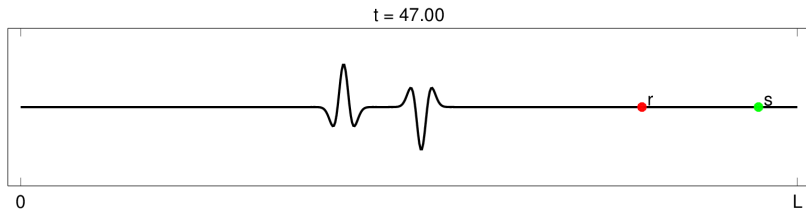


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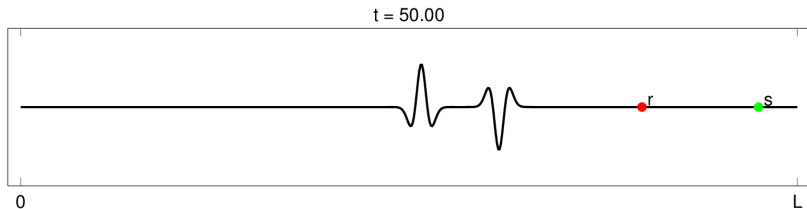


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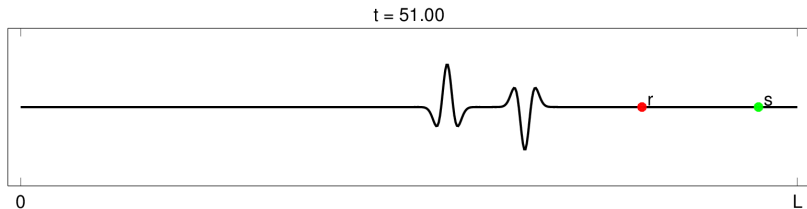


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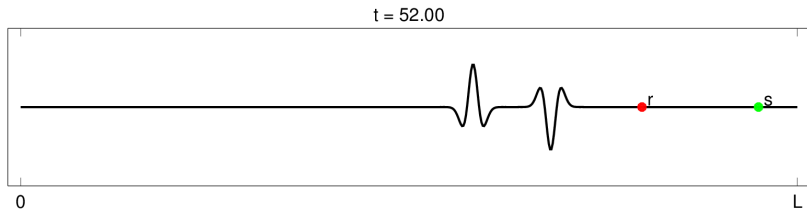


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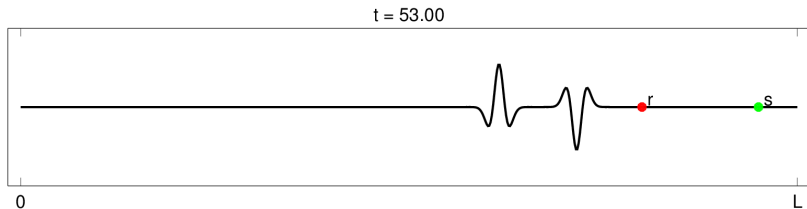


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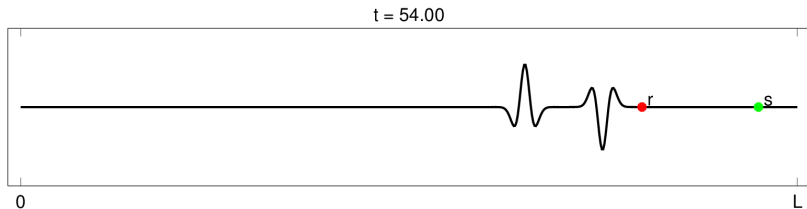


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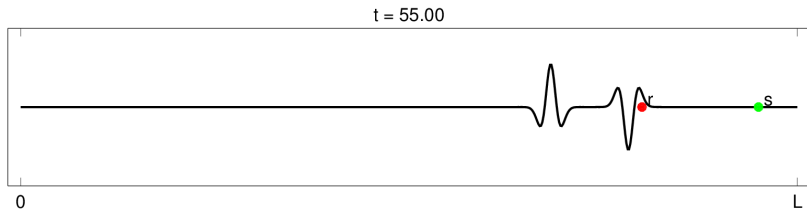


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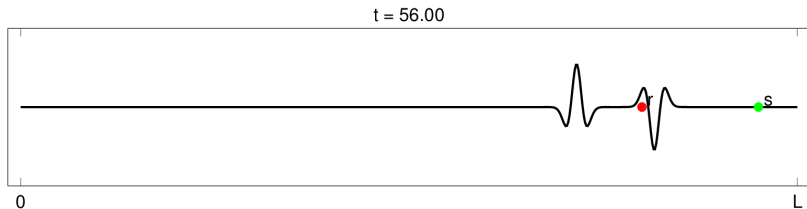


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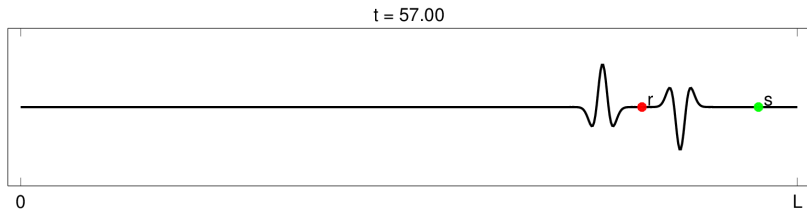


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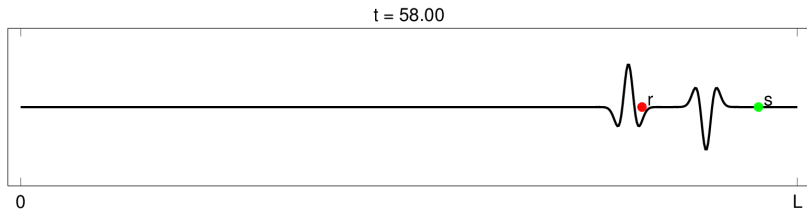


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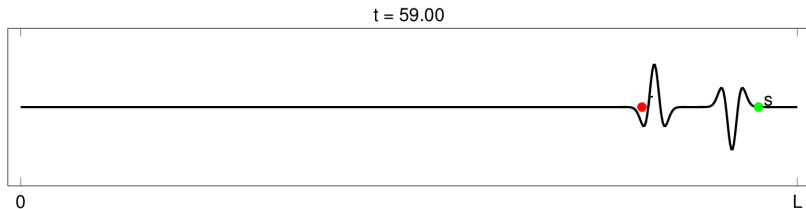


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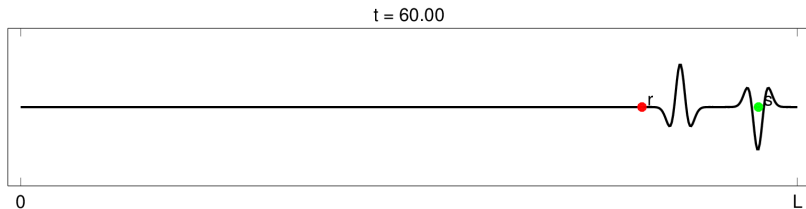


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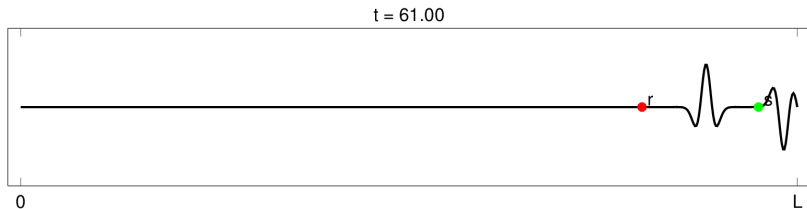


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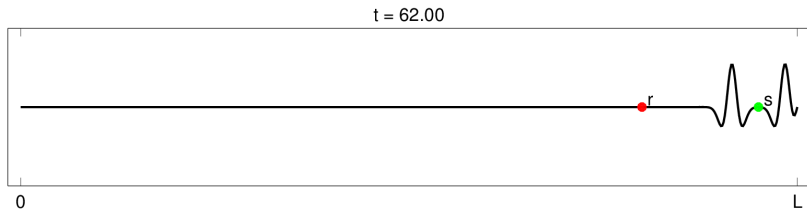


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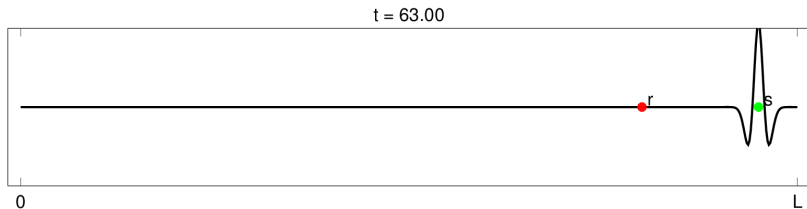


# Forward step

- The domain contains one source at  $x_s$  and one receiver at  $x_r$
- Simulated Numerically using a finite element method
- Wave propagation model

$$\frac{1}{c^2} \frac{\partial^2 p}{\partial t^2} - \frac{\partial^2 p}{\partial x^2} = f(t) \delta(x - x_s)$$

- Homogeneous Dirichlet boundary conditions and zero initial conditions
- Excitation function  $f(t)$  is a Ricker pulse centered at a known  $t_0$
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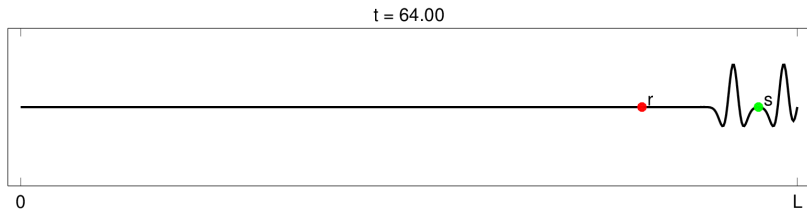


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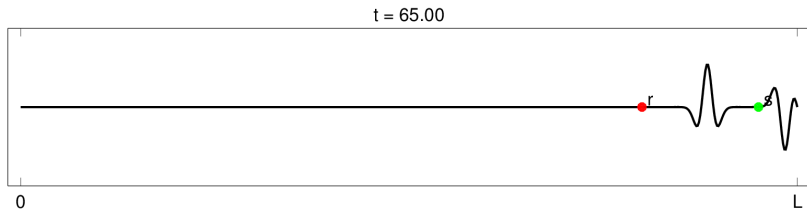


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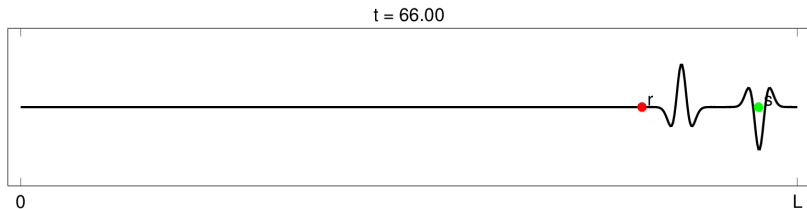


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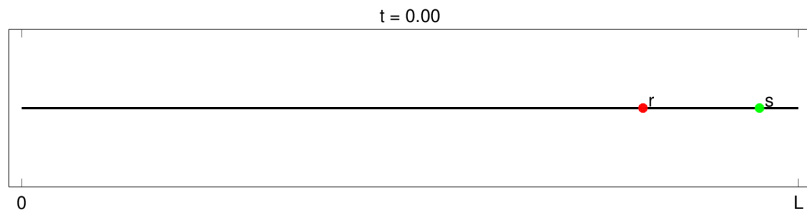


# Time domain solution - TR Backward step

- Always performed numerically
- The recorded signal is time reversed and retransmitted at  $x_r$

$$\frac{1}{c^2} \frac{\partial^2 p^{TR}}{\partial t^2} - \frac{\partial^2 p^{TR}}{\partial x^2} = p(x_r, T - t; x_s) \delta(x - x_r)$$

- Homogeneous Dirichlet boundary conditions and zero initial conditions
- Refocusing at time  $t_{RF} = T - t_0$
- Example with  $t_0 = 3.00$  and total time  $T = 66.00$

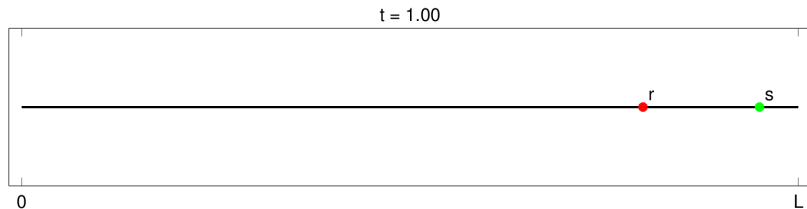


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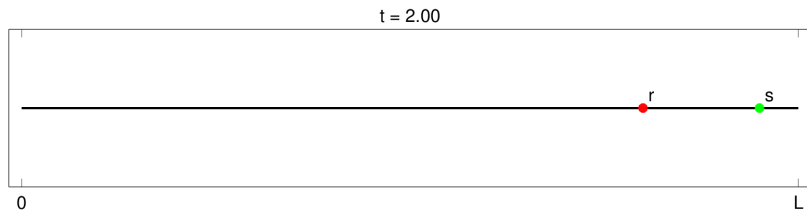


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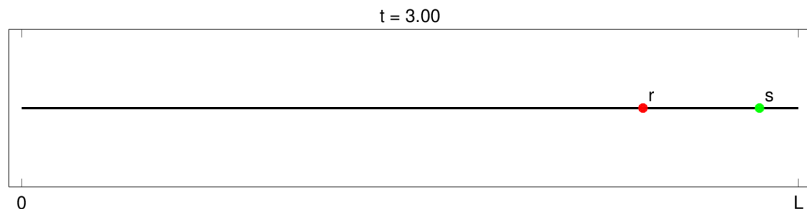


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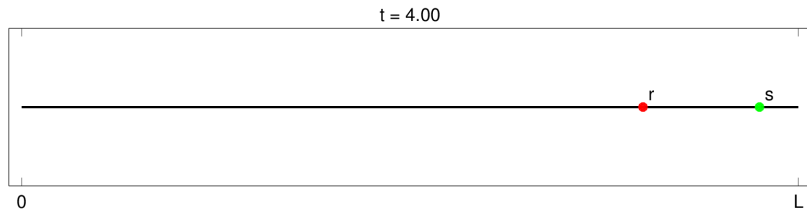


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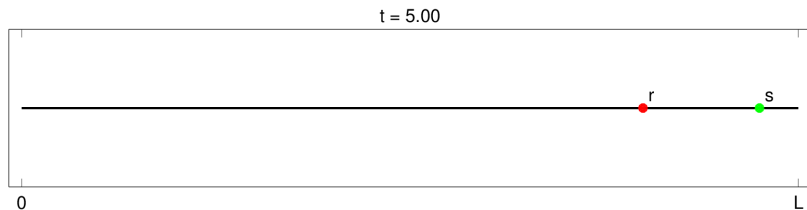


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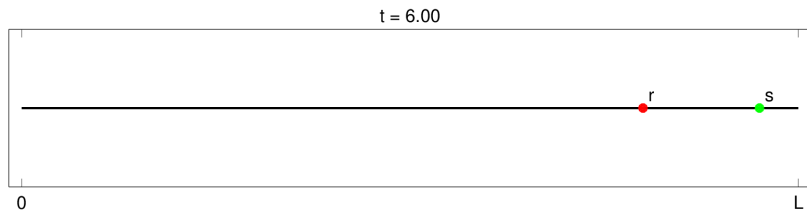


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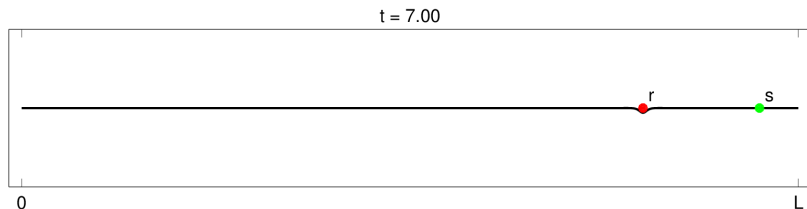


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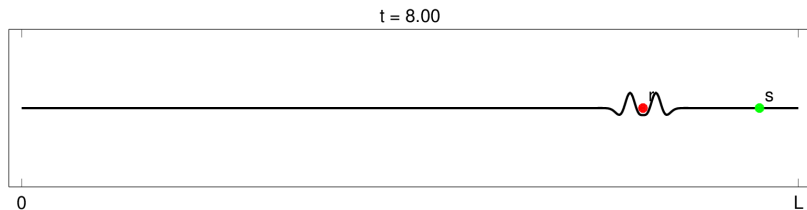


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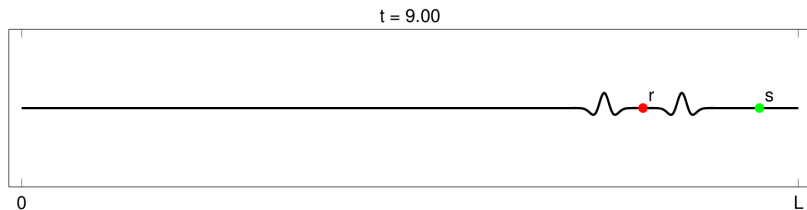


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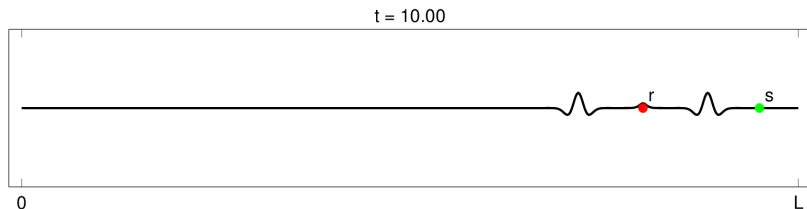


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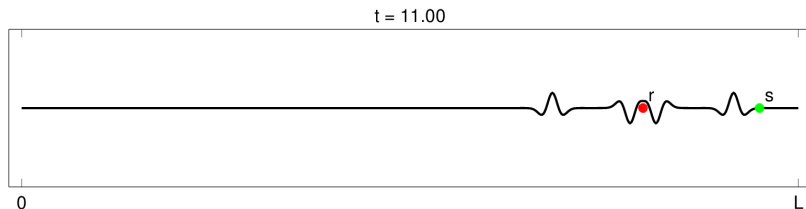


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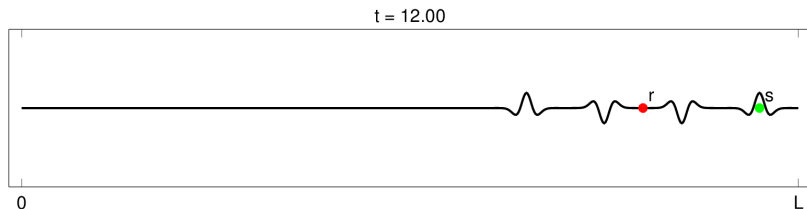


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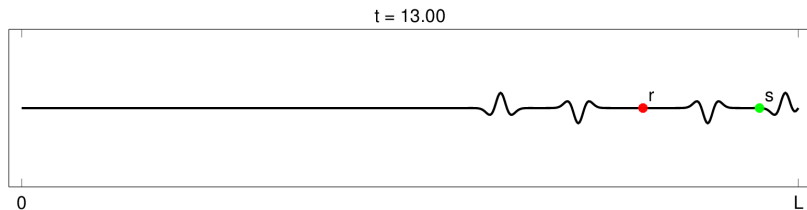


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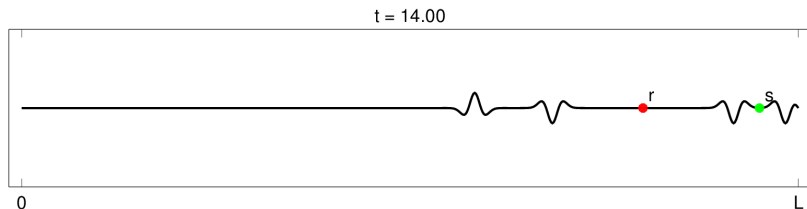


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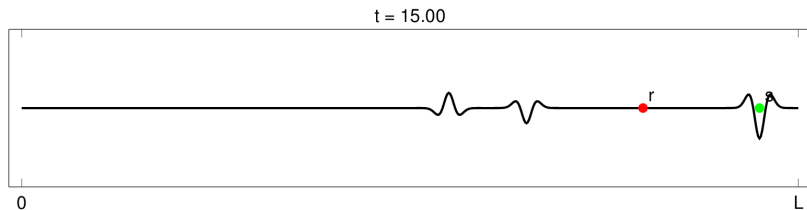


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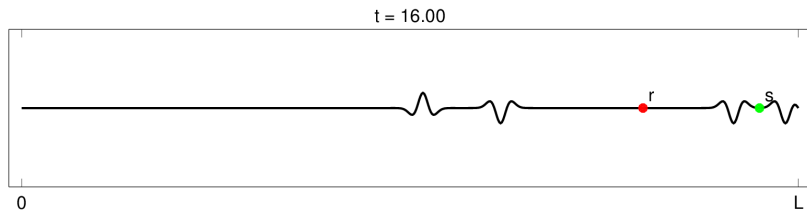


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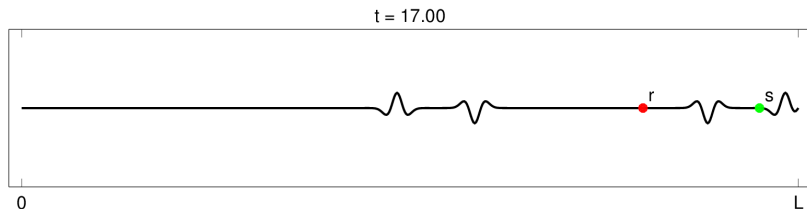


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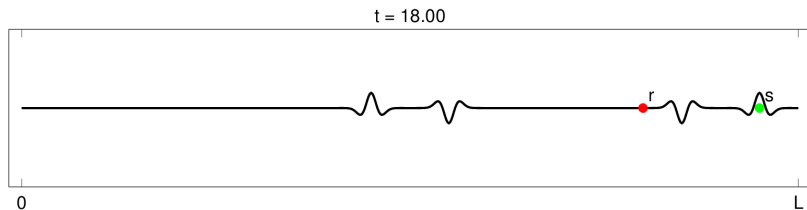


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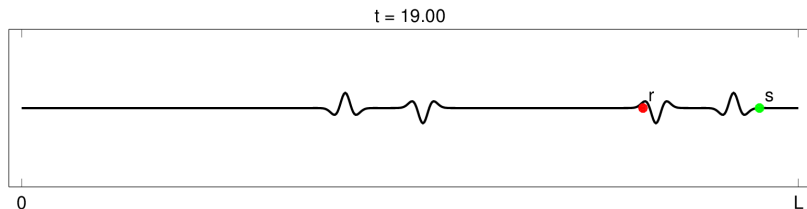


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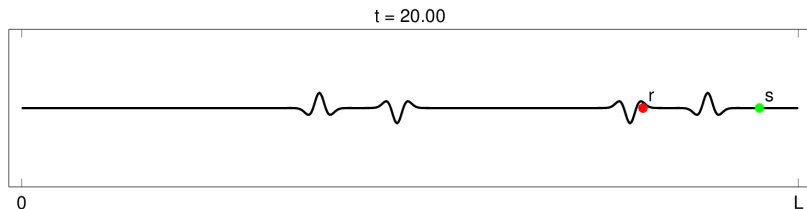


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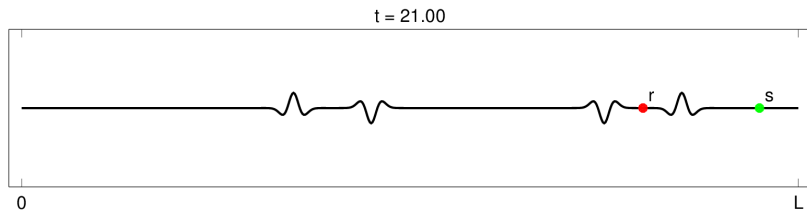


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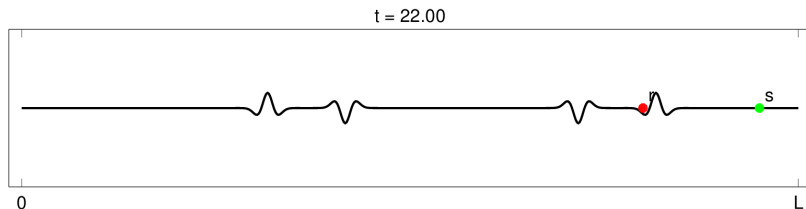


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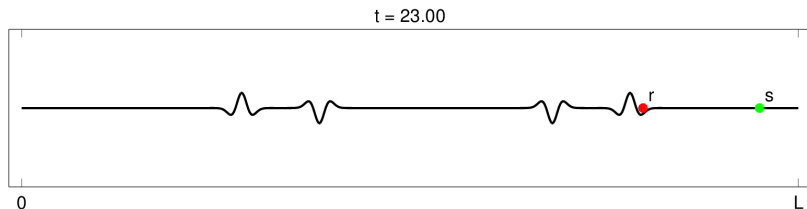


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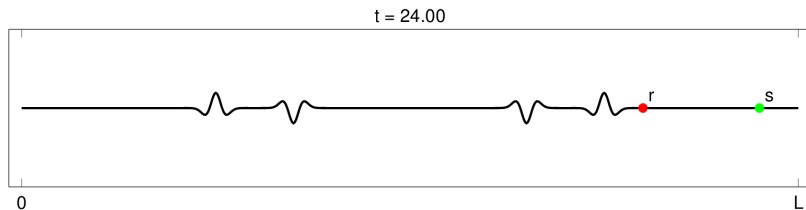


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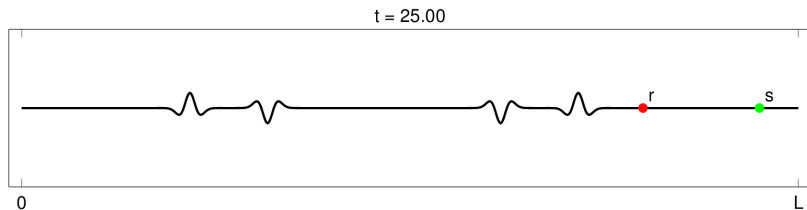


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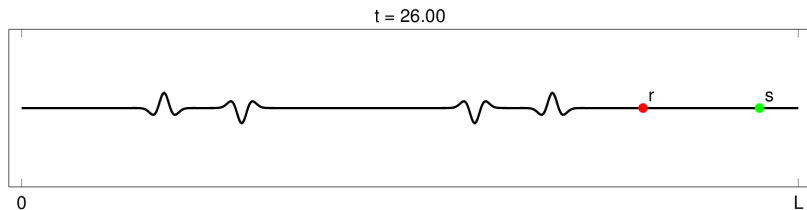


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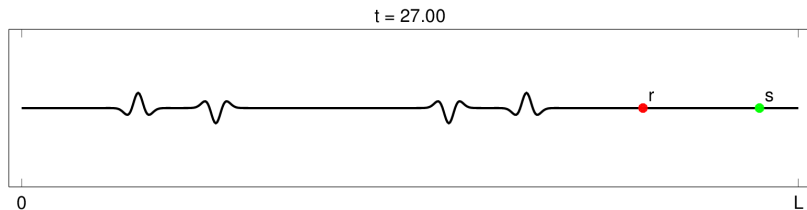


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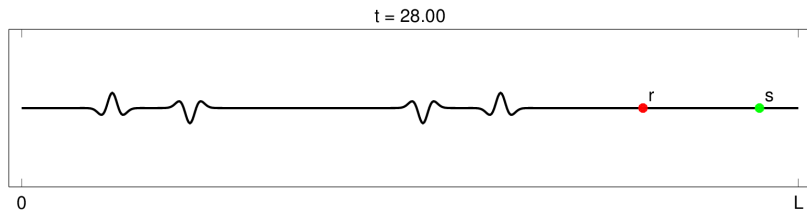


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- Refocusing at time  $t_{RF} = T - t_0$
- Example with  $t_0 = 3.00$  and total time  $T = 66.00$

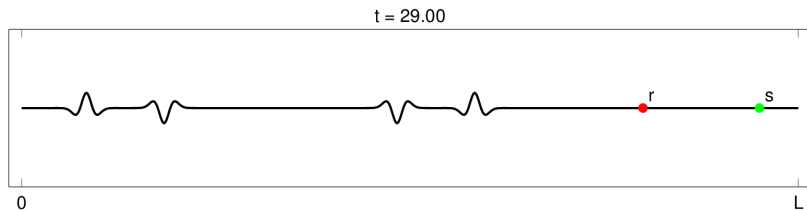


# Time domain solution - TR Backward step

- Always performed numerically
- The recorded signal is time reversed and retransmitted at  $x_r$

$$\frac{1}{c^2} \frac{\partial^2 p^{TR}}{\partial t^2} - \frac{\partial^2 p^{TR}}{\partial x^2} = p(x_r, T - t; x_s) \delta(x - x_r)$$

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- Example with  $t_0 = 3.00$  and total time  $T = 66.00$



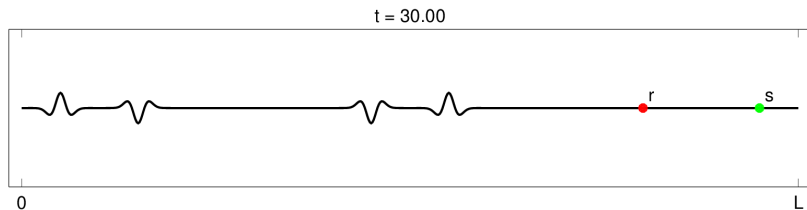


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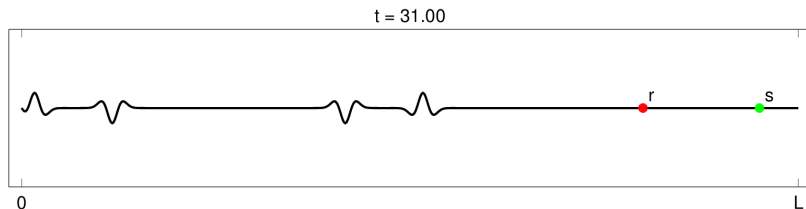


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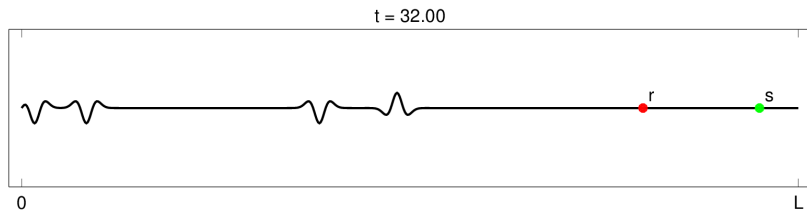


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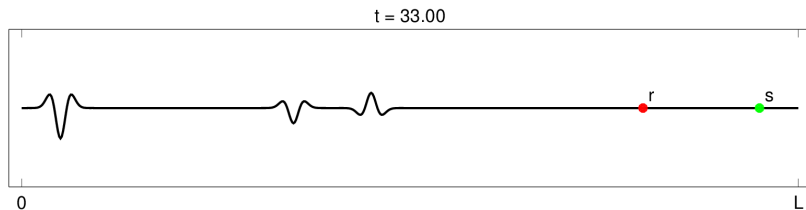


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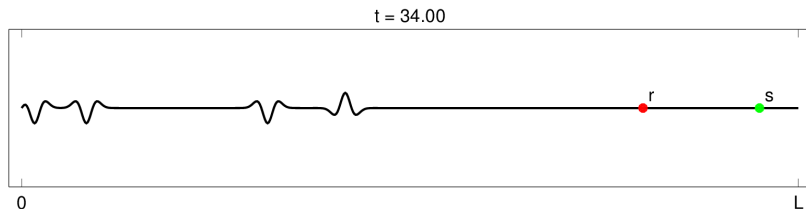


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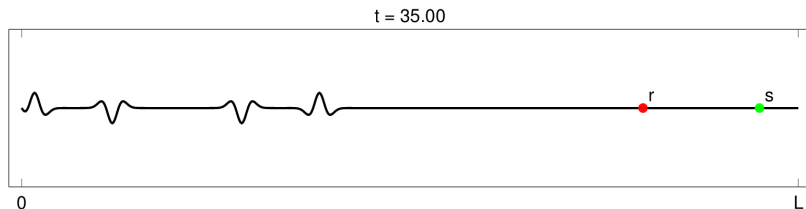


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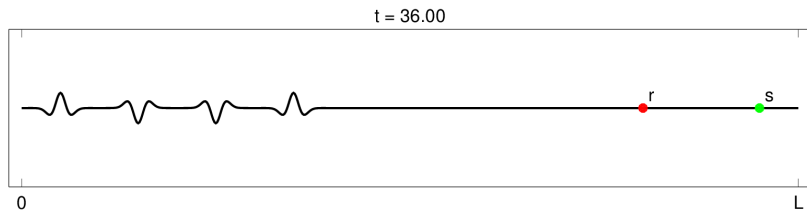


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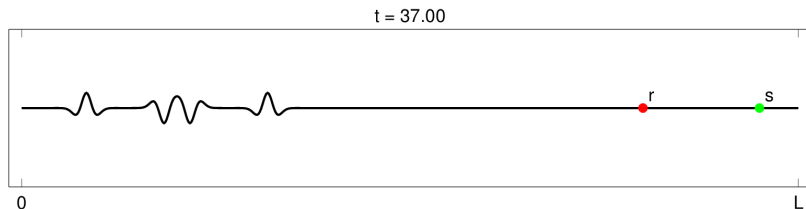


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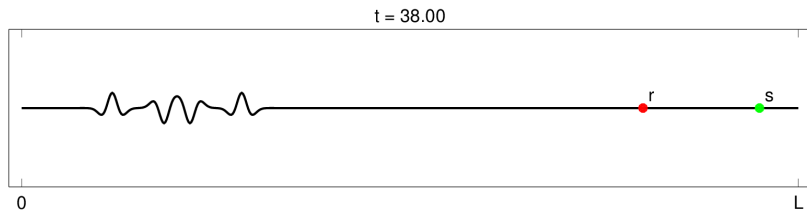


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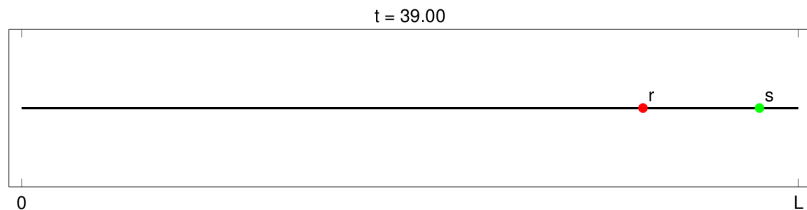


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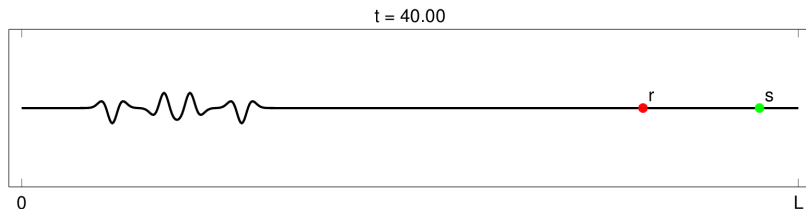


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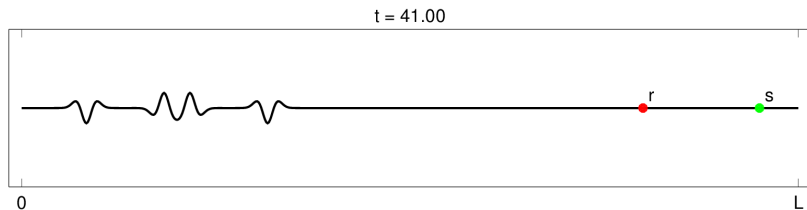


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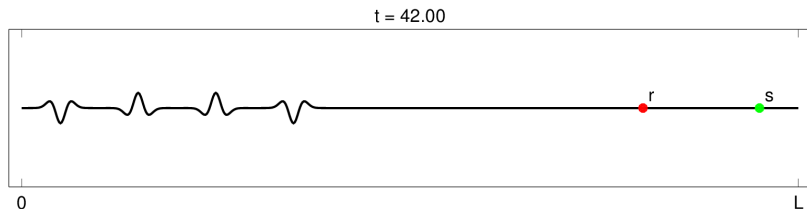


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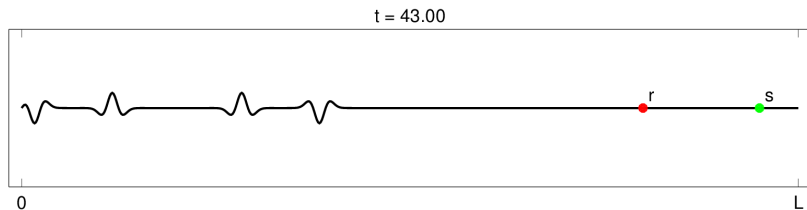


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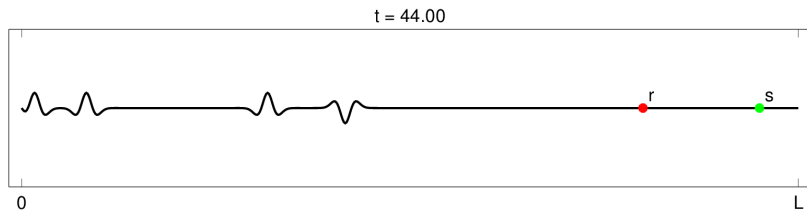


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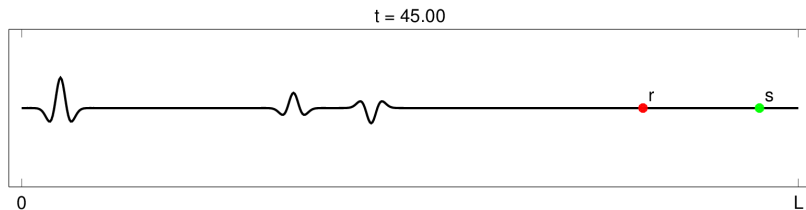


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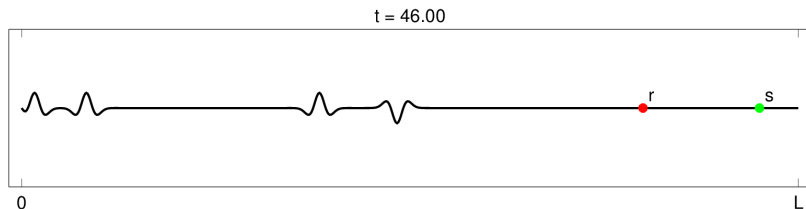


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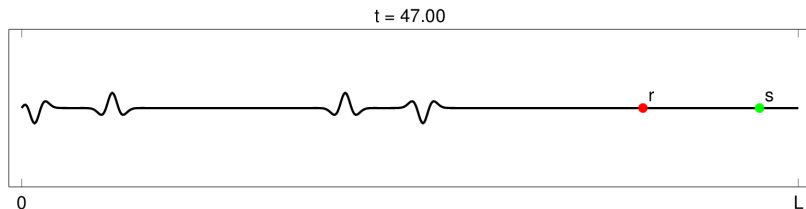


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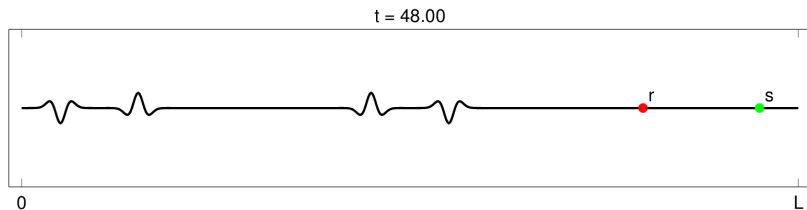


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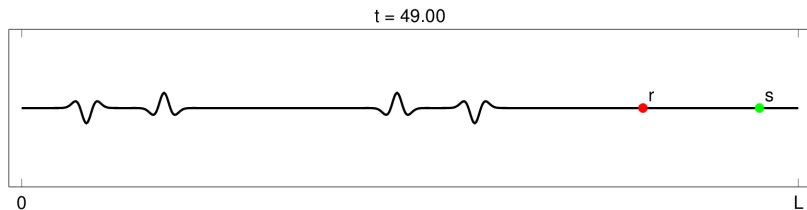


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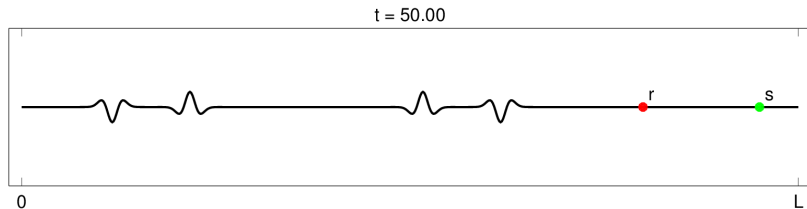


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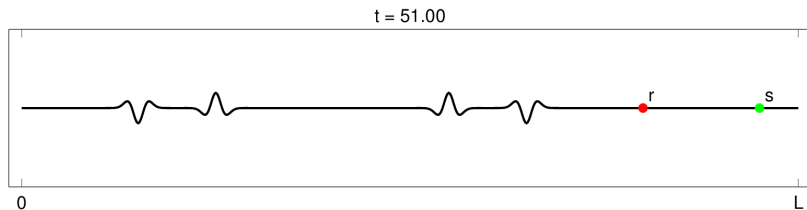


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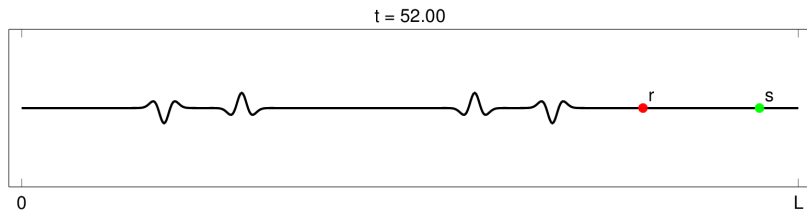


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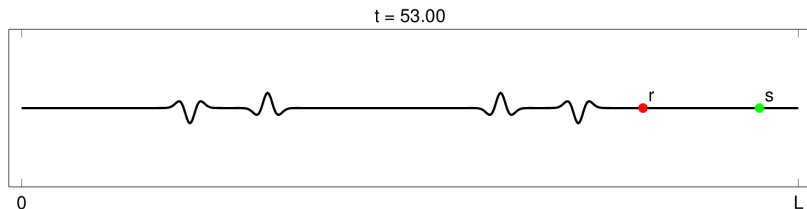


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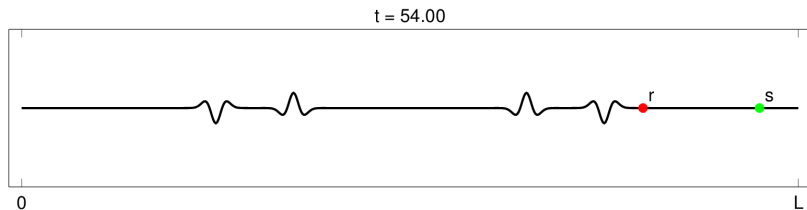


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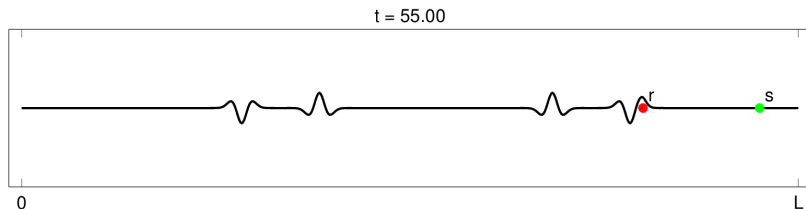


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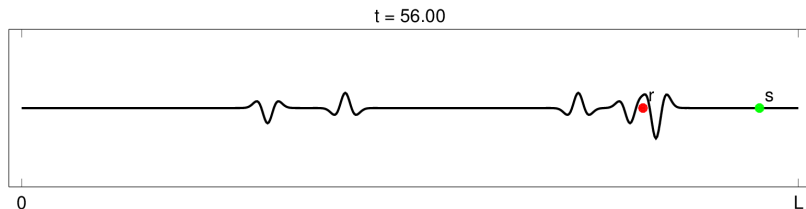


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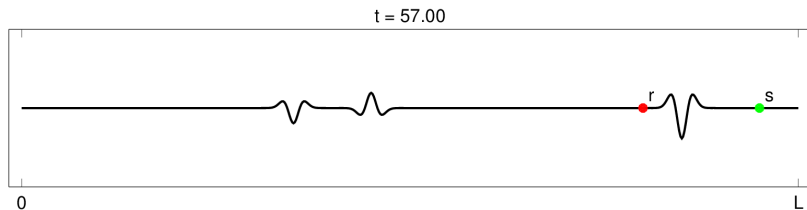


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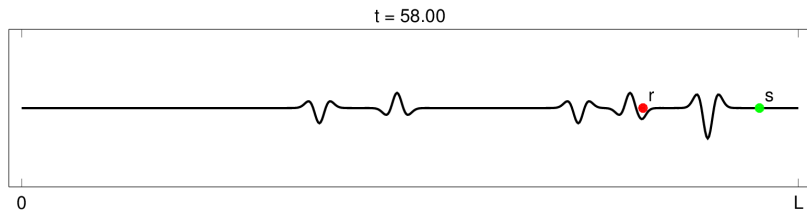


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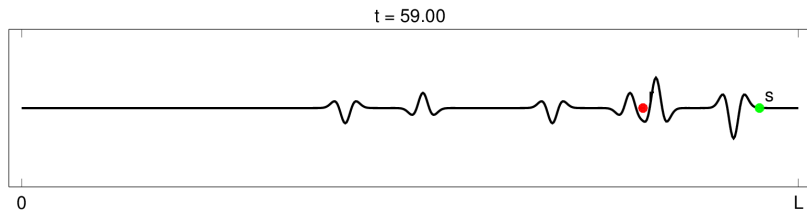


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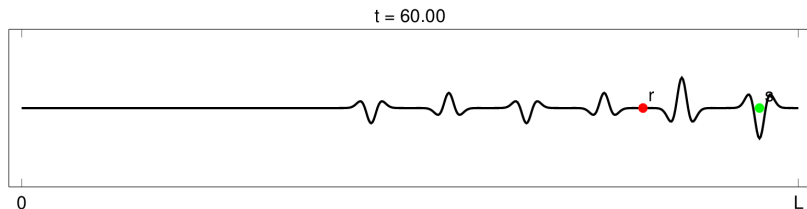


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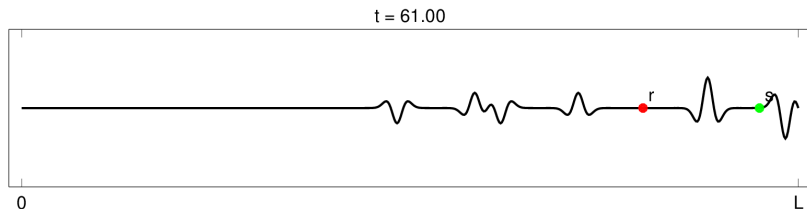


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- Always performed numerically
- The recorded signal is time reversed and retransmitted at  $x_r$

$$\frac{1}{c^2} \frac{\partial^2 p^{TR}}{\partial t^2} - \frac{\partial^2 p^{TR}}{\partial x^2} = p(x_r, T - t; x_s) \delta(x - x_r)$$

- Homogeneous Dirichlet boundary conditions and zero initial conditions
- Refocusing at time  $t_{RF} = T - t_0$
- Example with  $t_0 = 3.00$  and total time  $T = 66.00$



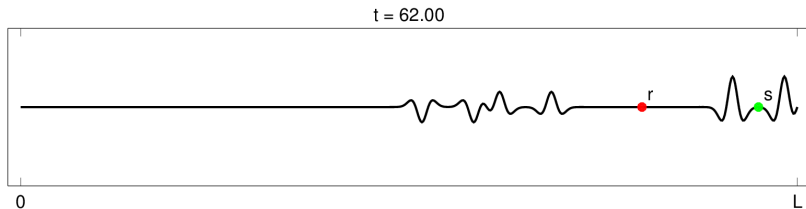


# Time domain solution - TR Backward step

- Always performed numerically
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$$\frac{1}{c^2} \frac{\partial^2 p^{TR}}{\partial t^2} - \frac{\partial^2 p^{TR}}{\partial x^2} = p(x_r, T - t; x_s) \delta(x - x_r)$$

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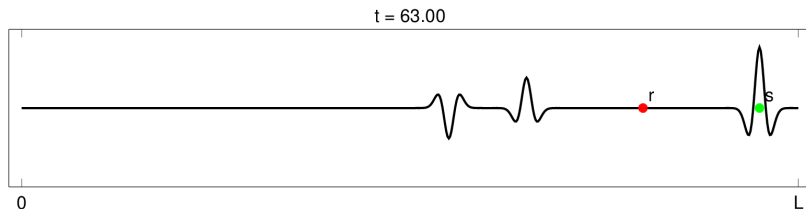


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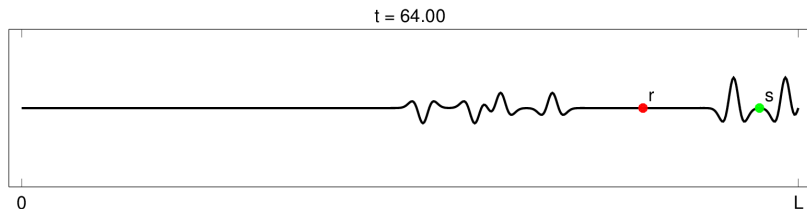


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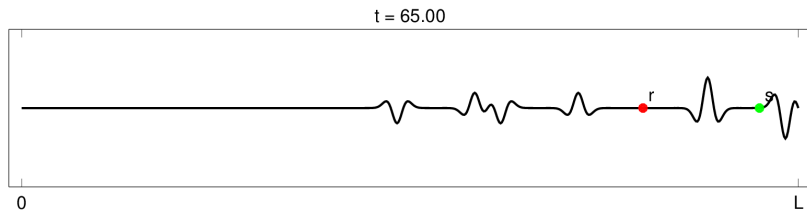


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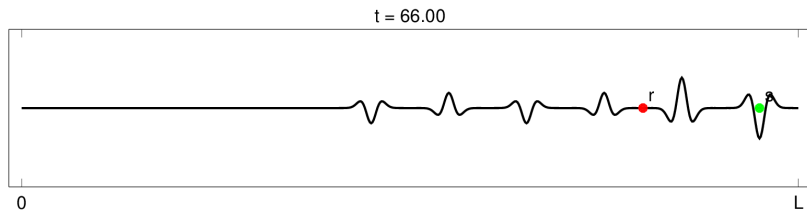


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# Frequency domain solution - Imaging

- Solution of the backward problem

$$F(x_r, t) = p(x_r, T - t) \Leftrightarrow \hat{F}(x_r, \omega) = \overline{\hat{p}(x_r, \omega)} e^{i\omega T}$$

# Frequency domain solution - Imaging

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$$p^{TR}(x, t) = F(x_r, t) \star_t G(x_r, x, t) = \frac{1}{2\pi} \int_{-\infty}^{\infty} \hat{F}(x_r, \omega) \hat{G}(x_r, x, \omega) d\omega$$



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- Evaluation of  $p^{TR}(x, t)$  at the refocusing time  $T - t_0$

$$p^{TR}(x, t = T - t_0) = \frac{1}{2\pi} \int_{-\infty}^{\infty} \overline{\hat{p}(x_r, \omega)} \hat{G}(x_r, x, \omega) e^{i\omega t_0} d\omega$$

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- Imaging functional - numerical approximation

$$I(x) = \frac{1}{2\pi} \sum_i \overline{\hat{p}(x_r, \omega_i)} \hat{G}^h(x_r, x, \omega) \Delta\omega_i$$

- Data at the receiver

$$p(x_r, t) = f(t) \star_t G(x_s, x_r, t) \Leftrightarrow \hat{p}(x_r, \omega) = \hat{f}(\omega) \hat{G}(x_s, x_r, \omega)$$

- Data at the receiver

$$p(x_r, t) = f(t) \star_t G(x_s, x_r, t) \Leftrightarrow \hat{p}(x_r, \omega) = \hat{f}(\omega) \hat{G}(x_s, x_r, \omega)$$

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- Substitute in the Imaging functional

$$I(x) = \frac{1}{2\pi} \sum_i |\hat{f}(\omega_i)|^2 \overline{\hat{G}(x_s, x_r, \omega_i)} \hat{G}(x_r, x, \omega) \Delta\omega_i$$

- Data at the receiver

$$p(x_r, t) = f(t) \star_t G(x_s, x_r, t) \Leftrightarrow \hat{p}(x_r, \omega) = \hat{f}(\omega) \hat{G}(x_s, x_r, \omega)$$

- Substitute in the Imaging functional

$$I(x) = \frac{1}{2\pi} \sum_i |\hat{f}(\omega_i)|^2 \overline{\hat{G}(x_s, x_r, \omega_i)} \hat{G}(x_r, x, \omega) \Delta\omega_i$$

- Modal expansion formula of the Green's function

$$G^{modal}(x, \xi, \omega) = \sum_{n=1}^N \frac{1}{\frac{\omega^2}{c^2} - \lambda_n} \Phi_n(x) \Phi_n(\xi)$$

# Modal expansion

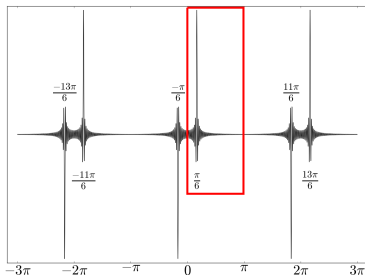
- After the calculations and omitting  $\hat{f}(\omega)$

$$\tilde{\text{I}}(x) = C_0 \sum_{i=1}^3 \left[ F_i \sum_{n=1}^N \sin\left(\frac{n\pi x}{L}\right) \sin\left(\frac{n\pi A_i}{L}\right) \right]$$

$i$	$F_i$	$A_i$
1	1.0	$x_s$
2	0.5	$x_s + 2x_r$
3	0.5	$x_s - 2x_r$

- Each of the series is a periodic (period  $2\pi$ ) that exhibits exactly one peak every half period

$$\sum_{n=1}^N \sin(nx) \sin(n\pi/6)$$





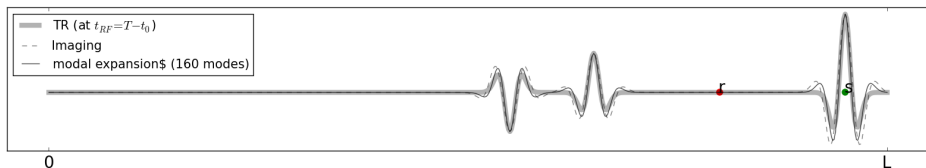
# Modal expansion

- After the calculations and omitting  $\hat{f}(\omega)$

$$\tilde{I}(x) = C_0 \sum_{i=1}^3 \left[ F_i \sum_{n=1}^N \sin\left(\frac{n\pi x}{L}\right) \sin\left(\frac{n\pi A_i}{L}\right) \right]$$

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- The imaging functional exhibits exactly three peaks within the interval  $[0, L]$



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# Time domain solution - TR

- source, receiver and 1 defect - small area around  $x_d$  with different wave velocity
- each time the original pulse passes from the defect it splits into a transmitted and a reflected component
- Assumption : the incident field  $p_{inc}$  is known (the response at the healthy domain)
- scattered field  $p_{scat} = p_{tot} - p_{inc}$  to minimize the influence of the source
- The defect acts as a multiple in time source
- $p_{scat}$  is time reversed and retransmitted
- not only one refocusing time but the strongest at  $t^{RF} = T - t_1 - t_0$

- Data at the receiver - Born approximation

$$\hat{p}_{scat}(x_r, \omega) = k^2 \hat{f}(\omega) \rho \hat{G}(x_s, x_d, \omega) \hat{G}(x_d, x_r, \omega) \quad (1)$$

- It seems natural to define an imaging functional as

$$I(x) = \sum_i \overline{\hat{p}_{scat}(x_r, \omega)} \hat{G}^h(x_r, x, \omega) \hat{G}^h(x, x_s, \omega) \quad (2)$$

- The appearance of the two Green's functions differentiates imaging from TR
- results from the two methods are not comparable unlike the source localization

- Substituting  $\hat{G}^h$  and  $\hat{p}_{scat}$  into the Born approximation

$$I(x) = \sum_{\omega} k^2 \rho \left( \hat{f}^h(\omega) \right)^2 \overline{\hat{f}(\omega) \hat{G}(x_s, x_d, \omega) \hat{G}(x_d, x_r, \omega) \hat{G}(x_r, x, \omega) \hat{G}(x, x_s, \omega)}$$

- Using the modal expansion of  $\hat{G}$

$$\tilde{I}(x) = C_1 \left\{ \sum_{i=1}^{13} \left[ F_i \sum_{n=1}^N \cos\left(\frac{2n\pi x}{L}\right) \cos\left(\frac{2n\pi A_i}{L}\right) \right] + \sum_{n=1}^N \cos\left(\frac{2n\pi x}{L}\right) \right\} + C_2$$

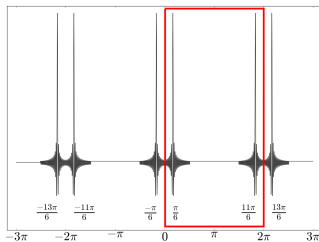
# Modal expansion

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$i$	$F_i$	$A_i$	$i$	$F_i$	$A_i$	$i$	$F_i$	$A_i$	$i$	$F_i$	$A_i$
1	1.0	$x_d$	4	0.5	$x_d - x_s$	7	0.5	$x_d + x_r$	10	0.25	$x_d - x_s - x_r$
2	1.0	$x_s$	5	0.5	$x_d + x_s$	8	0.5	$x_s - x_r$	11	0.25	$x_d - x_s + x_r$
3	1.0	$x_r$	6	0.5	$x_d - x_r$	9	0.5	$x_s + x_r$	12	0.25	$x_d + x_s - x_r$
									13	0.25	$x_d + x_s + x_r$

- Each of the series is a periodic (period  $2\pi$ ) that exhibits exactly two peaks in every period

$$\sum_{n=1}^N \cos(nx) \cos(n\pi/6)$$

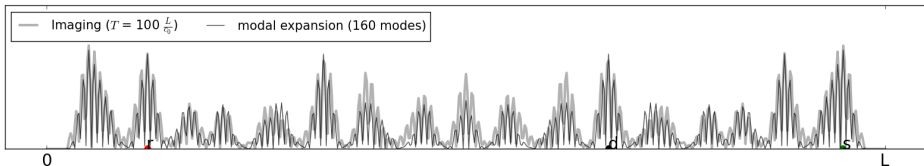


# Modal expansion

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- The imaging functional exhibits exactly 26 peaks within the interval  $[0, L]$

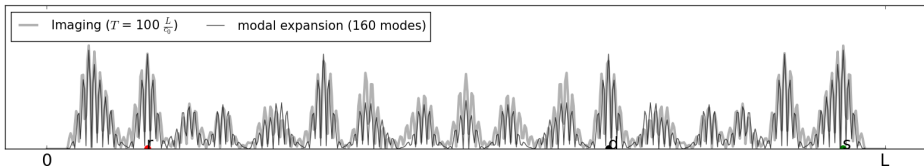


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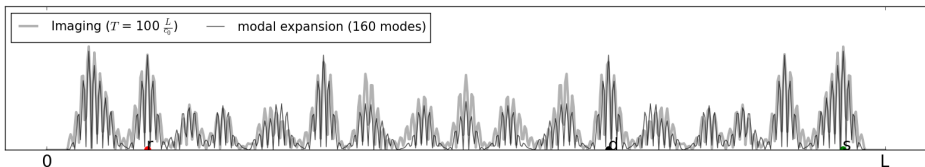


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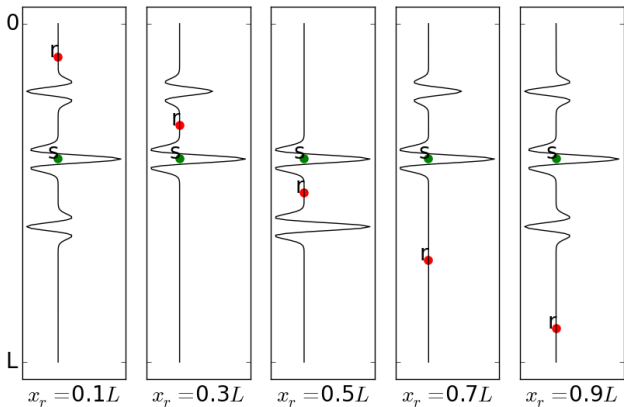
- In defect localization the choice of  $T$  is of significant importance
- Time reversal
  - If the wave travels many times across the domain,  $p_{scat}$  becomes complicated
  - Best results for  $T = \frac{|x_s - x_d|}{c_{ref}} + \frac{|x_d - x_r|}{c_{ref}} + 2t_0$
  - Because  $x_d$  is not known, optimum choice  $T = \frac{2L}{c_{ref}} + 2t_0$
- Imaging
  - The data at the receiver and Green's functions are calculated in the time domain and then FT
  - As a result  $T$  can be taken into account similarly to the TR case
- Modal expansion
  - It is assumed here that  $T = \infty$  and thus no further discussion is meaningful
  - If Imaging is performed for very large  $T (\rightarrow \infty)$  it approaches the modal expansion

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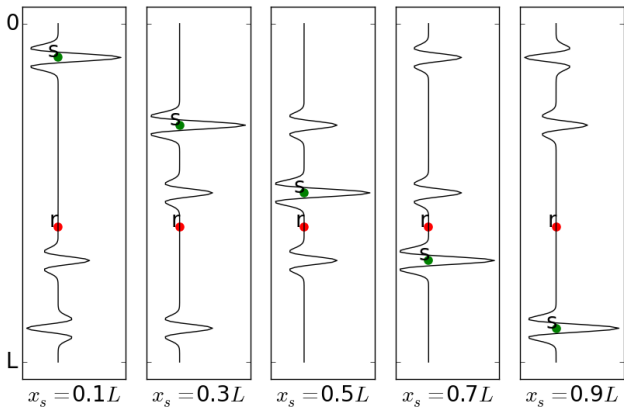
# Source localization - Imaging

- Investigation of the receiver position



# Source localization - Imaging

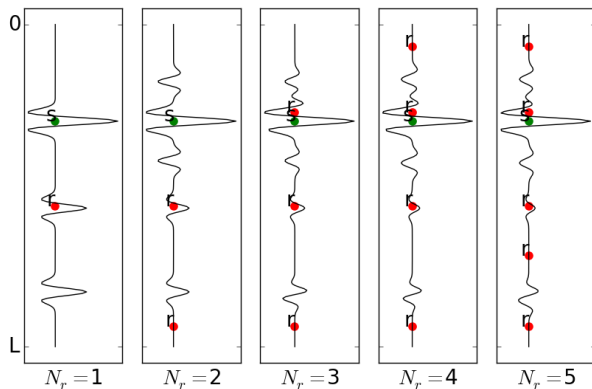
- Investigation of the source position



# Source localization - Imaging

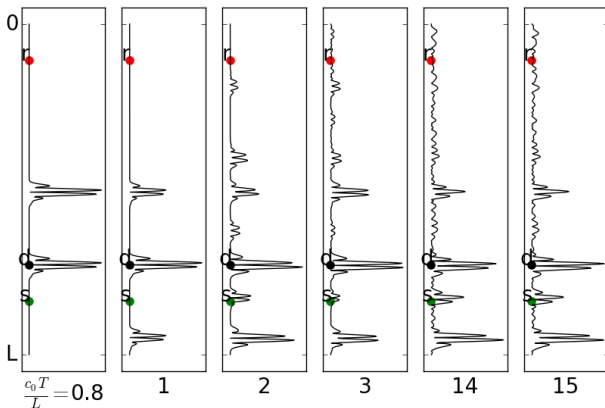
- Improvement of the SNR by increasing the number of receivers
- Linear relationship between SNR and  $N_r$

$$I(x) = \sum_{\omega} \sum_{r=1}^{N_r} \overline{\hat{p}(x_r, \omega)} \hat{G}^h(x_r, x, \omega). \quad (3)$$



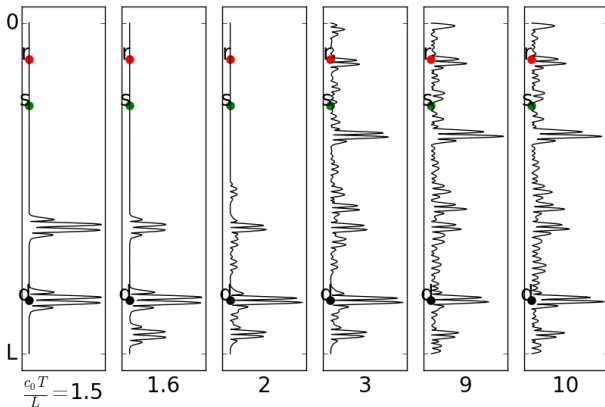
# Defect localization - TR

- Time reversal for defect localization example 1
- Investigation of total experiment time  $T$



# Defect localization - TR

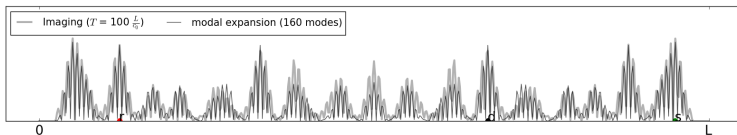
- Time reversal for defect localization example 2
- Investigation of total experiment time  $T$



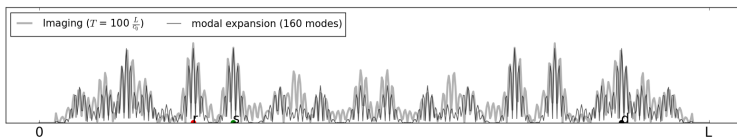


# Defect localization - Imaging and modal expansion

- Comparison of Imaging ( $T=\infty$ ) and modal expansion
- Example 1



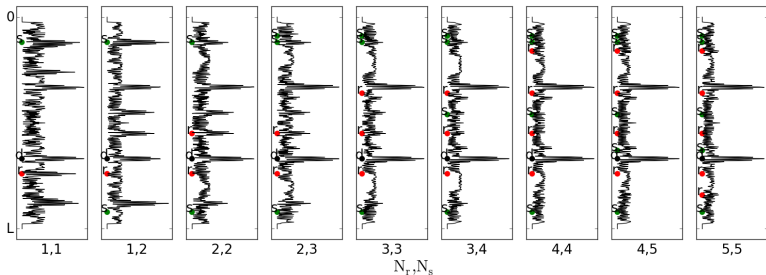
- Example 2



# Defect localization - Imaging

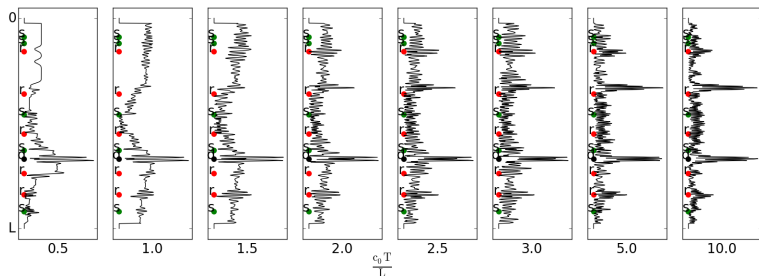
- Improvement of the image quality using higher number of sources and receivers

$$I(x) = \sum_{\omega} \sum_{r=1}^{N_r} \sum_{s=1}^{N_s} \widehat{p}_{scat}(x_r, \omega) \widehat{G}^h(x_r, x, \omega) \widehat{G}^h(x, x_s, \omega) \quad (4)$$



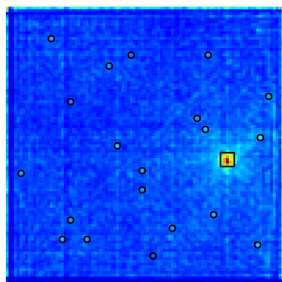
# Defect localization - Imaging

- Improvement of the SNR by reducing total time  $T$

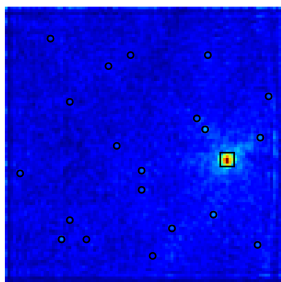


# Defect localization 2D example - Imaging

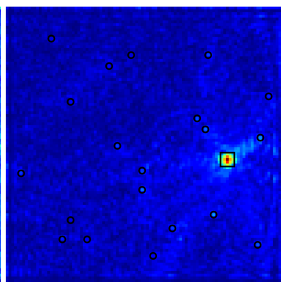
- 2D bounded domain, contains 20 receivers that act as sources as well
- Investigation of the total experiment time
- Much better results compared to the 1D case because :
  - In the 1D case the defect separates the domain in two parts
  - Large number of receivers and sources



$$T = 10 \frac{\sqrt{2}L}{c_0}$$



$$T = 4 \frac{\sqrt{2}L}{c_0}$$



$$T = 2 \frac{\sqrt{2}L}{c_0}$$

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# Summary and Conclusions

- TR and Imaging for damage localization in 1D acoustic bounded media
- Exploitation of the similarities and disparities between source and defect localization problems
- Analyzed the noise resulting from the presence of the boundaries
- Investigated the effect of the total experiment time  $T$
- Proposition of techniques for the improvement of SNR and image quality
- Results from defect localization in 2D domain are very promising

- Extend the Imaging techniques in elastic media and higher dimensions
- Investigate the localization process for noisy recordings
- Utilize passive only recordings due to ambient vibration
- Apply techniques for the separate localization of multiple defects<sup>5</sup>
- Apply this methodology on structures with complex geometry<sup>6</sup> for the development of SHM systems

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5. CG Panagiotopoulos, Y Petromichelakis, C Tsogka (2015) Time Reversal in elastodynamics and applications to Structural Health Monitoring, COMPDYN 2015

6. CG Panagiotopoulos, Y Petromichelakis, C Tsogka (2015) Time reversal and imaging for structures, Chapter in "Dynamic Response of Infrastructure to Environmentally Induced Loads"[\[1\]](#)